

# ECG signal Noise removal technique with new Thresholding and adaptive filter

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**Abstract:** Electrocardiogram signals are one for biomedical signals, which reflects electrical activity for heart. ECG signals are widely studied & applied in clinic. ECG signals is obtained by recording produced by an electrocardiographic device & collected by skin electrodes placed at designated locations on body. ECG signal is defined by six peaks & valleys, which are traditionally labeled P, R, Q, S, T & U. Aim for thesis is to remove noise inside the ECG signal & to calculate parameters just to signal like signal to noise ratio (SNR) & root means square error (RMSE). In this technique, when we decompose a data set using wavelet, we use filters that act as averaging filters & others that produce details. few for resulting wavelet coefficients corresponds to detail in data set. If details are small, they might be omitted without substantially affecting main features for data set. Then thresholding is used to set to zero all coefficients that are less than particular threshold. These coefficients are used in an inverse wavelet transformation to reconstruct data set. Hence with help for WT noise is removed from ECG signal.

**Keywords:** DSP: Digital Signal Processing, RMSE: root means square error, db: Daubechies wavelets, sym: symlet wavelet, LMS: Least Mean Square

## I-INTRODUCTION

Digital Signal Processing has become an useful tool in a multitude for diverse fields for science & technology. In field of digital signal processing has grown enormously in past decade to encompass & provide firm theoretical backgrounds just to a large number for individual areas. ECG varies with respect to time, need in order to obtain an accurate description for ECG different frequency contents as per their location on time is must. This justifies use for time and frequency presentation in a quantitative electro cardiology. Immediate tool available in order to isolate frequency and time a Short Term Fourier Transform (STFT). However major draw-back for STFT is it time & frequency precision is not quite optimal. Hence we need a much suitable method to overcome this problem. Among different time & frequency transformations the wavelet Transformation found to be easy & much valuable. wavelet transformation based on set for analyzing wavelets which allows decomposition for ECG signal into a set for coefficients. Every analyzing wavelet has their own time duration and time location & frequency band. Wavelet coefficient producing from wavelet transformation also corresponds to measurement for ECG components at that time segment & frequency band. ECG signals noise are:-

**Electromyography noise** - arises from superposition for muscular electric potentials over ECG signal whereas

wideband noise is associated with imperfections in electronic circuitry involved with ECG acquisition in totality **Power line interference** - is attributed to improper shielding for ECG acquisition devices from power supply & imperfections in amplifier circuitry.

**Baseline wondrous**- Baseline wander results from change in electrode impedance due to perspiration & motion for patient.

**Electromagnetic interference** - from other electronic devices & noise coupled from other electronic devices, usually at high frequencies.

**Motion artifact** - comes from variation for electrode-skin contact impedance.

**Additive White Gaussian Noise (AWGN)** - which has a Gaussian probability density function & white power spectral density function (noise distributed over entire frequency spectrum) & is linearly added to whatever signal we are analyzing.

**Denosing Procedure:** normal de-noising method involves three basic steps. Basic version for procedure follows steps described As.

**First Decompose** - select a wavelet; select a level N. Compute wavelet decomposition for signal s at that level N.

**Second Threshold detail coefficients** - in order to every level from 1 to N, select a threshold & apply soft or hard thresholding [13][13]to detail coefficients.

**Third Reconstruct** - Calculate wavelet reconstruction with the help of actual approximation coefficients for level N & modified detail co-efficients for levels from 1 to N. 1.2

## II-LITERATURE SURVEY

M. Butt et al. [2] proposed a new shrinkage function in order to denoising ECG signal & compared results with various shrinkage functions. Their proposed procedure gives better results, proposed procedure shows a new experimental threshold value in order to each decomposition level for wavelet coefficients, better MSE & SNR values comparative to hard- & soft- thresholding methods, they use wavelet & chose appropriate threshold from available threshold methods. M. Rosu, et al. [1] have evaluated performances for four various threshold estimators rules in application for denoising ECG signal in MATLAB7 environment. They proposed an efficient wavelet based shrinkage procedure to filter out power line frequency. According to authors proposed algorithm is easy to implement in real time application, involves less computational complexity & gives better visual display. They also treated EEG signal as noise component & applied wavelet shrinkage algorithm to remove EEG from ECG signal. simulated results show that

universal procedure performs better at all SNR. They derive their own new formula in order to finding appropriate threshold value & filtered according that.

### III-IMPLEMENTATION

The basic idea behind this thesis is estimation for uncorrupted ECG signal from corrupted or noisy signal, & is also referred to as “signal denoising”. There are various methods to help restore ECG from noisy signal corrupted by various noises. Selecting Appropriate procedure plays a major role in getting desired ECG signal. denoising methods tend to be problem specific. in order to example a procedure that is used to denoise audio signal may not be suitable in order to denoising medical signals. Audio signals are stationary in nature whereas ECG signals are non stationary or time varying signals. In this thesis, a study is made on various thresholding & shrinkage functions are used in order to denoising signal & implemented in MATLAB. Proposed procedure is compared with various thresholding & shrinkage functions in terms for its SNR & RMSE. In order to quantify performance for various denoising algorithms, a simulative ECG is taken & few known noise in order to example Additive White Gaussian(AWG) is added to it. This would then be given as input to Denoising algorithm, which produces ECG signal close to original ECG signal performance for proposed procedure is compared by computing Signal to Noise Ratio (SNR) & Root Mean Square Error (RMSE).

General de-noising procedure involves three steps. basic version for procedure follows steps described below.

**Decompose:** Choose a wavelet, choose a level N. Compute wavelet decomposition for signal s at level N. **Threshold detail coefficients:** in order to each level from 1 to N, select a threshold & apply soft thresholding [12] to detail coefficients. **Reconstruct:** Compute wavelet reconstruction using original approximation coefficients for level N & modified detail coefficients for levels from 1 to N.

While registering ECG signal it may get contaminated by random noises uncorrelated with ECG signal. These noises may be approximated by white Gaussian noise. Thresholding is used in wavelet domain to smooth out or to remove few coefficients for wavelet transform for sub signals for measured signal. This reduces noise content for signal under non-stationary environment. proposed procedure is implemented using following steps.

**Step1:** ECG signal may be develop with help for MATLAB function. Let it is  $x(n)$

**Step2:** add random & adaptive white Gaussian noise with various quantity for noise to ECG signal. White Gaussian noise with zero mean & constant variation is generated & added to noise free ECG signal. Mathematically this may be written as

$$y(n) = x(n) + w(n)$$

Where,  $x(n)$  is noise free ECG signal,  $w(n)$  is white Gaussian noise &  $y(n)$  is noisy ECG signal.

**Step 3:** apply LMS adaptive filter in order to filter out unexpected shape from noisy ECG signal. Adaptive filters works on behalf for its available ideal shape for ECG & remove all unexpected shapes.

$$z(n) = \text{filt}_{\text{LMS}}(x(n))$$

**Step 4:** Using an appropriate mother wavelet in our case symlet with order 6, to noisy ECG signal is decomposed to obtain approximate & detailed coefficients.

$$\{Z_L(\omega), Z_H(\omega)\} = \text{Sym}\{z(n)\}$$

**Step 5:** Choose a threshold value in order to thresholding. Selection for threshold value plays an important role in denoising for ECG signal. A number for methods in order to threshold estimation have been proposed. Thesis work,evaluated performance for following threshold estimators on denoising for ECG signal.

**(a) Universal Thresholding:** This is proposed by Donoho. threshold value T is given by

$$T = \sqrt{2 * \log(n)}$$

where, n is number for samples in signal.

**(b) Hard Thresholding:** In 1995 Donoho developed hard shrinkage function & given by formula

$$\hat{Y} = \begin{cases} 0 & |Y| < T \\ Y & |Y| > T \end{cases}$$

Hard thresholding is simplest method. hard thresholding [13]can be described as usual procedure for setting to zero elements whose absolute values are lower than threshold. soft thresholding [12]is an extension for hard thresholding, first setting to zero elements whose absolute values are lower than threshold, & then shrinking nonzero coefficients towards 0.As may be seen in comment for figure, hard procedure creates discontinuities at  $Y = \pm T$

**(c) Soft thresholding:** In 1995 Johnston developed soft shrinkage function & given by formula

$$\hat{Y} = \begin{cases} 0 & |Y| < T \\ Y - T & Y > T \\ Y + T & Y < -T \end{cases}$$

In soft thresholding, in addition to that remaining coefficients are also reduced linearly. soft thresholding [12][12]is an extension for hard thresholding, first setting to zero elements whose absolute values are lower than threshold, & then shrinking nonzero coefficients towards 0.

**(d) Firm Thresholding:** derivation for standard soft shrinkage function is not continuous. Both hard & soft shrinkages have advantages & disadvantages. soft shrinkage estimates tend to have a bigger bias, due to shrinkage for large coefficients. Due to discontinuities for shrinkage function, hard shrinkage estimates tend to have a bigger variance. In other words, it will be sensitive to small changes in signal. To overcome drawbacks for hard & soft shrinkage,

a firm shrinkage function was introduced by Gao & Bruce & given by formula

$$\hat{Y} = \begin{cases} 0 & |Y| \leq T_L \\ \text{sgn}(Y) \left[ \frac{T_H(|Y-T_L|)}{(|Y-T_L|)} \right] & T_L < |Y| < T_H \\ Y & |Y| > T_H \end{cases}$$

Where, T2 is decided by formula (1), scope for T1 is 0~T2. According to previous experiments when T1 equals 2/3T2, denoised results would be better. Shrinkage function is continuous & approaches identity line as |Y| increase. firm shrinkage function provides a good compromise between hard & soft shrinkage function.

The firm shrinkage is less sensitive than hard shrinkage to small fluctuations & less biased than soft shrinkage.

**(e) Yasser thresholding:** In 2006 Yasser presented an improved threshold shrinkage function as formula (5).(named Yasser shrinkage function) & given by formula

$$\hat{Y} = \begin{cases} Y & |Y| \geq T \\ \text{sgn}(Y) \cdot \frac{|Y|^\gamma}{T^{\gamma-1}} & |Y| < T \end{cases}$$

Where, value for T is decided by formula given by Donoho. Yasser shrinkage just shrinks wavelets coefficients which are lower than threshold & it keep continuing for function.  $\gamma=3$  was used to finish speech signals denoising & obtained good results.

The shrinkage expressed by firm & Yasser, combined advantages for hard shrinkage with soft shrinkage, possess better results in signal denoising. however it wasn't designed in order to ECG signal specially & could not obtain best result in denoising processing. in order to firm shrinkage, denoised result for ECG signal is closely to hard shrinkage when contamination is slight. in order to Yasser shrinkage, denoised signal can't be smooth enough when contamination is serious.

**(f) Proposed thresholding method:** A new shrinkage function was proposed in this thesis. parameters for this shrinkage function were optimized by comparing denoised results for simulative ECG signal at various contaminating levels. In order to verify denoised results for presented shrinkage conveniently, symlets wavelet (sym6), 5-level & global thresholding were used in order to whole denoising process. choice for threshold & shrinkage function is most important step in order to wavelet denoising. In order to obtain best denoising results, a new shrinkage function which would be used in ECG signals denoising was proposed here, expressed as formula

$$\hat{Y} = \begin{cases} 0 & |Y| \leq T_L \\ \text{sgn}(Y) \left[ \frac{|Y - T_L|^\gamma \cdot T_H}{|T_H - T_L|^\gamma} \right] & T_L < |Y| \leq T_H \\ Y & |Y| > T_H \end{cases}$$

Obviously, shrinkage function expressed in above formula synthesized many formats. following work is to figure out a best format which may produce best denoising result in order to ECG signal.

**Step 6:** After estimating threshold values, apply thresholding to shrinkage wavelet detailed coefficient for noisy signal. Normally there are two types for thresholding methods, hard thresholding [13][13]and soft thresholding. In hard thresholding [13][13]all coefficients below threshold value are set to zero. however in soft thresholding, in addition to that remaining coefficients are also reduced linearly.

**Step 7:** After thresholding compute inverse discrete wavelet transform to estimate original ECG signal.

**Step 8:** To evaluate performance for proposed method, Signal to Noise Ratio(SNR) & Root mean square error (RMSE) between original signal & estimated signal is computed.

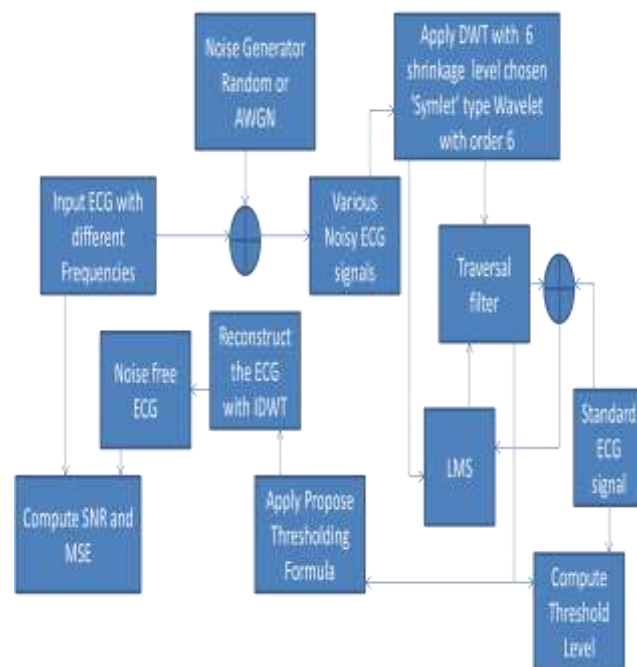


Figure 1 Proposed system

#### IV-RESULTS

The Codes are written in order to hard threshold, soft threshold, firm threshold, Yasser threshold & Proposed thresholding & shrinkage functions. These codes are simulated, synthesized & implemented in MATLAB2012b.

results for simulation are reported here. images which are obtained are as follows:-

first, as shown in Fig 2 ECG signal containing 2048 sampling points. P wave, QRS wave, ST wave, T wave & U wave all have been described precisely. amplitude & frequency for simulative ECG signal are similar to real one. Generally clinical ECG signals always contain noise (however contamination is slight). ECG signal is been mixed up with adaptive white Gaussian noise signal.

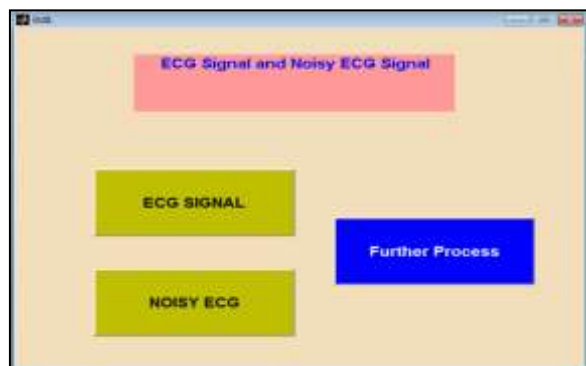


Figure. 2 GUI in order to ECG signal & noisy ECG signal generation

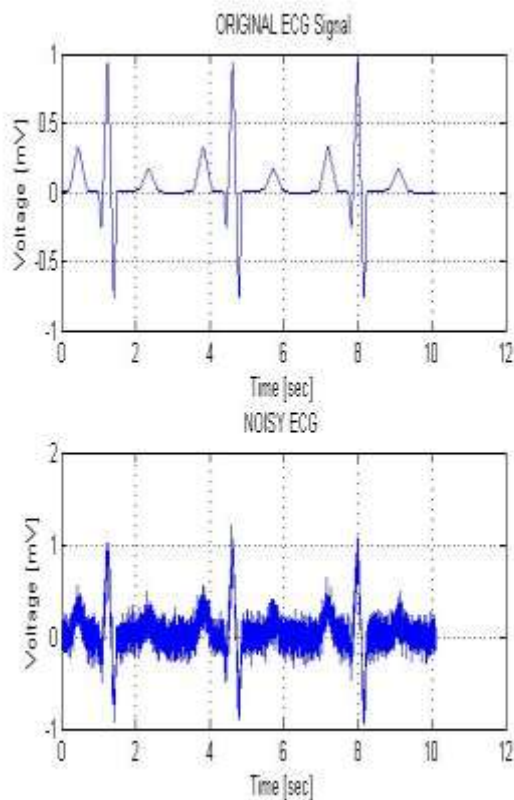


Figure 3 Original ECG and noisy signal

The AWGN noise is added to ECG signal & this signal is now considered as noisy ECG & denoise by applying DWT, thresholding & IDWT. threshold selected is proposed threshold.



Figure 4 Proposed ECG filter output

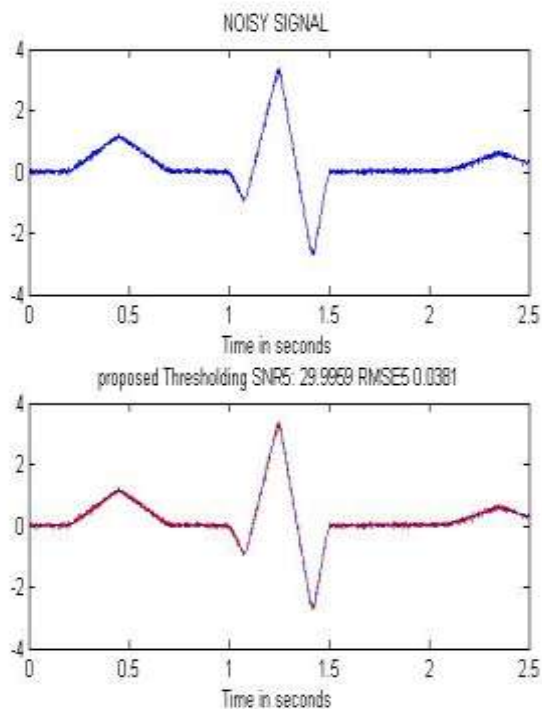


Figure 5 Recover ECG

Figure 5 MATLAB figure window shows denoise ECG signal by Proposed thresholding method. The figure shows above denoise signal with proposed thresholding. signal to noise ratio & root mean square error are shown in MATLAB

figure window. As shown in above figure blue line is noise free signal & red line is denoise signal.

The final results for Signal to Noise Ratio (SNR) & Root Mean Square Error (RMSE) for these methods are summarized as shown in following table:-

Thresholding Methods	SNR in dbs	RMSE
Hard threshold	25.9022	0.040959
Soft threshold	26.2878	0.039186
Firm threshold	26.3486	0.0389071
Yasser threshold	26.085	0.040106
M. Rosu, et al. [1]	25.43	NA
M. Butt et al. [2]	16.24	0.062854
Proposed threshold	29.9053	0.038455

**Table 1 Comparative results**

it may be observe that both SNR & RMSE are better than other four standard methods that are Yasser, Firm, hard & soft thresholding respectively also proposed work RMSE is less than base work M. Rosu, et al. [1] & base work for M. Butt et al. [2] & PSNR observed in proposed work is 29.90 which is higher than available works, hence proposed ECG will have good similarities & smoothness.

### V-CONCLUSION

The proposed threshold & shrinkage function is useful while processing ECG signal & to improve signal-to-noise ratio (SNR) in order to obtaining clean recordings & preserve original shape for signal, especially peaks, without distorting waves & segments. main job is to recover a true ECG signal from noisy recording & successfully achieved by proposed method. Proposed procedure looks also to be rather versatile. While it originated as a tool in order to signal separation, its use has expanded way beyond this field; it has been used relatively early in order to problems such as noise reduction in ECG signal processing, analyzing ECG in clinic. speed for operation for algorithm may be improved by using an enhanced algorithm. database enrichment may be achieved from MIT BIH physionet. database collected from MIT BIH treated as problem & that signals may simply loaded in order to analyzing that data, series for algorithm on various signals from various domains. study for ECG signal interfered by various noises may be denoised with help for proposed procedure which will efficiently denoised signal corrupted by various noises. in order to analyzing simulated ECG signal we have added AWGN, which is uniformly corrupts that signal. & that signal is denoised by proposed method.

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